Efficient Solution Methods for Inverse Problems with Application to Tomography Practical Tomography

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Content



Imaging Systems and Mathematical Models







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Content



2 Fan Beam Geometry

3 3D X rays



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Transmission Tomography

- X-Ray CT (Nobel Prize 1979)
- Phase Contrast Tomography
- Magnetic Resonance Imaging (Nuclear Magnetic Resonance; Nobel Prize 2003)
- Ultrasound CT
- Electromagnetic Waves
- Impedance
- Light
- Electron Paramagnetic Resonance Imaging
- Transmission Electron Microscopy

Emission Tomography

- PET
- SPECT
- EEG / MEG

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Bioluminescence Imaging

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Nondestructive Testing

Nondestructive Testing

- X-Ray CT
- Ultrasound
- Microwaves
- Backscattering X-Ray CT
- Synchrotron Rays
- Phase Contrast Tomography
- Transmission Electron Microscopy



Historical Image

Leonardo da Vinci, 1500



Leonardo da Vinci. Anatomische Zeichnung. Um 1500



Historical Image

Hand of Dean of Röntgen, A.v. Koelliker, 23.01.1896



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X-Ray CT





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Fan Beam Geometry

$$\mathsf{D}f(a,\theta) = \int_0^\infty f(a+t\theta)dt$$

Relation to Radon transorm

 $\mathbf{D}f = U\mathbf{R}f$

where U is a unitary transform.

Transformation of the parallel geometry inversion to fan beam inversion.



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2 Fan Beam Geometry





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3D X rays

Basics



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Typical Scanning Geometry in NDT



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• 3D Radon Transform: $\mathbf{R}f(\theta, s) = \int_{\theta^{\perp}} f(s\theta + y) dy$



• 3D Radon Transform: $\mathbf{R}f(\theta, s) = \int_{\theta^{\perp}} f(s\theta + y) dy$ Inversion Formula

$$f(x) = -rac{1}{8\pi^2}\int_{\mathcal{S}^2} (\mathbf{R}f)''(heta, x^ op heta)d heta$$



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• 3D Parallel X - Ray Transform $\mathbf{P}f(\theta, y) = \int_{-\infty}^{\infty} f(y + t\theta) dt$



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$$f = c \mathbf{P}^* \mathbf{I}^{-1} \mathbf{P} f$$

where

$$\mathbf{I}^{-1}g(\xi) = |\xi|\hat{g}(\xi)$$

and

$$\mathbf{P}^*g(x)=\int_{\mathcal{S}^2}g(heta,E_ heta x)d heta$$

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Too many data!

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Synchrotron Measurements

Parallel X - Ray Transform for $\theta \in S^1 \times \{0\}$. Then Transform

$$\mathbf{P} = \mathbf{P}_2 \otimes \mathbf{I}$$

Adapt 2D-Inversion (B. Hahn)

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3D Synchrotron Data





Better results using 3D algorthms: Bernadette HAHN



Big Challenge

Application: Determination of fluid flow in porous media



Big Challenge

Application: Determination of fluid flow in porous media Object time dependent



Big Challenge

Application: Determination of fluid flow in porous media Object time dependent

Data inconsistent for classical transform



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Source position: $a \in \Gamma$ Direction: $\theta \in S^2$



Source position: $a \in \Gamma$ Direction: $\theta \in S^2$

$$\mathsf{D}f(a,\theta) = \int_0^\infty f(a+t\theta)dt$$

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Source position: $a \in \Gamma$ Direction: $\theta \in S^2$

$$\mathsf{D}f(a,\theta) = \int_0^\infty f(a+t\theta)dt$$

For flat detectors use other geometry



Source position: $a \in \Gamma$ Direction: $\theta \in S^2$

$$\mathbf{D}f(a,\theta) = \int_0^\infty f(a+t\theta)dt$$

For flat detectors use other geometry Compare with Radon transform in \mathbb{R}^3

$$\mathbf{R}f(\omega, s) = \int f(x)\delta(s - x^{\top}\omega)dx$$

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Dual Transform

$$oldsymbol{\mathsf{D}}: L_2(\mathbb{R}^3) o L_2(\Gamma imes S^2)$$
 $oldsymbol{\mathsf{D}}^*g(x) = \int_{\Gamma} |x-a|^{-2}g\Big(a, rac{x-a}{|x-a|}\Big) da$

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Relation between Radon and Cone Beam Transform

Grangeat:

$$\frac{\partial}{\partial s} \mathbf{R} f(\omega, \boldsymbol{a}^\top \omega) = -\int \mathbf{D} f(\boldsymbol{a}, \theta) \delta'(\omega^\top \theta) d\theta$$

Proof:

$$\int \mathbf{R} f(\omega, s) \psi(s) ds = \int f(x) \psi(x^{\top} \omega) dx$$
$$\int \mathbf{D} f(a, \theta) h(\theta) d\theta = \int f(x) h\left(\frac{x-a}{|x-a|}\right) |x-a|^{-2} dx$$

Put $\psi(s) = \delta'(s - a^{\top}\omega)$ and $h(\theta) = \delta'(\theta^{\top}\omega)$ and use δ' homog. of degree -2 in \mathbb{R}^3 .



References

- Hamaker, Smith, Solmon, Wagner, 1980
- Tuy, 1984
- Grangeat 1986
- Dietz 1999
- AKL, 2000
- Katsevich, 2000
- Zhao, Jiang, Zhuang, Wang, 2006
- ...

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Inversion Formula

Theorem (AKL 2004)

Let the condition of Tuy-Kirillov be fulfilled. Then the Inversion formula can be given as



Inversion Formula

Theorem (AKL 2004)

Let the condition of Tuy-Kirillov be fulfilled. Then the Inversion formula can be given as

$$f=-rac{1}{8\pi^2}D^*TM_{\Gamma,a}TDf$$

where

$$egin{aligned} D^*g(x) &= \int_{\Gamma} |x-a|^{-2}g(a,rac{x-a}{|x-a}) da \ Tg(\omega) &= \int_{S^2} g(heta) \delta'(heta^ op \omega) d heta \ M_{\Gamma,a}h(\omega) &= |a'^ op \omega| m(\omega,a^ op \omega) h(\omega) \end{aligned}$$

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Crofton Symbol

m = 1/*n*

where *n* is the Crofton symbol, counting how often a plane trhough a point cuts the source path Γ Hence $n \in \mathbb{N}_0$ and therefore *m* is not differentiable!

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Challenge

Inversion formula contains detailed information about curve Γ . But in practice measurements are taken only at discrete points. How to include in algorithms?



3D X rays

Images





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Images





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Reconstruction Kernel



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Data from DKFZ





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Reconstruction





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Surprise Egg



3D X rays



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Data from IzfP





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• Katsevich uses π - lines



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- hence integration over parts of Γ where *n* is constant

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- Backprojection depends on reconstruction point x



- Katsevich uses π lines
- hence integration over parts of Γ where *n* is constant
- Backprojection depends on reconstruction point *x*
- Jump of *n* at the end introduces δ distributions, hence point evaluation of data

Application for example: printed circuit board

Data given in very small range

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- Classical Algorithms fail

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Application for example: printed circuit board

- Data given in very small range
- Classical Algorithms fail
- So far: Iterative algorithms realized on graphical processors (GPU)
- Optimizing order of used equations
- Use a priori information (see Lavrentiev)

Importance of Mathematics





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